

FEM multigrid techniques for the simulation of fluid-structure interaction with application to hemodynamics

H. Damanik, M. Razzaq, A. Ouazzi, S. Turek, Department of Applied Mathematics, LS III, TU Dortmund http://www.featflow.de

Numerical Analysis and Scientific Computing with Applications May 18-22, 2009 Agadir, Morocco



A. Ouazzi | NASCA 2009, Agadir

Fluid structure interaction



- Deformation of a structure in internal/external flow
- Model for bioengineering
- Numerical methods
- Benchmarking



FSI experiment vs numerical simulation





Brain Aneurysms and stent implants



Problem Description

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Structure part

Fluid part

$$\chi^{s}: \Omega^{s} \times [0, T] \mapsto \Omega^{s}_{t}$$
$$u^{s} = \chi(X, t) - X, \quad v^{s} = \frac{\partial u^{s}}{\partial t}$$
$$F = I + \nabla u^{s}, \quad J = \det(F)$$

$$\chi^{f}: \Omega^{f} \times [0, T] \mapsto \Omega^{f}_{t}$$
$$u^{f} = \chi(X, t) - X$$
$$v^{f}: \Omega^{f} \times [0, T] \mapsto \mathbb{R}^{n}$$





$$\chi: \Omega \times [0,T] \mapsto \Omega_t; \qquad v = \frac{\partial \chi}{\partial t}, \qquad F = \frac{\partial \chi}{\partial X}, \qquad J = \det(F)$$
$$\chi_R: R \times [0,T] \mapsto R_t, \quad R \subset \Omega_t \,\forall t \in [0,T]; \quad v_R = \frac{\partial \chi_R}{\partial t}, \qquad F_R = \frac{\partial \chi_R}{\partial X}, \quad J_R = \det(F_R)$$

$$\frac{\partial}{\partial t} \int_{R_t} p dv + \int_{\partial R_t} \rho \left(v - v_R \right) \cdot n_{R_t} da = 0$$
$$\frac{\partial}{\partial t} \left(\rho J \right) + \nabla \cdot \left(\rho J_R \left(v - v_R \right) F^{-T} \right) = 0$$

Lagrangian description

Eulerian description

$$\xi_R = \chi \Longrightarrow F_R = F, \ J_R = J, \ v_R = v \quad \xi_R = Id \Longrightarrow F_R = I, \ J_R = 1, \ v_R = 0$$
$$\frac{\partial}{\partial t} \left(\rho J\right) = 0 \qquad \qquad \frac{\partial\rho}{\partial t} + \nabla \cdot \left(\rho v\right) = 0$$



Coupling Strategies

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Weak coupling (separated)

Strong coupling (separated)

> Monolithic

tⁿ Fluid & Solid
$$\rightarrow$$
 tⁿ⁺¹ Fluid & Solid



Discrete Nonlinear System



$$R(X) = 0, X = (u_h, v_h, p) \in U_h \times V_h \times P_h$$

$$\frac{\partial R}{\partial X}(X) = \begin{bmatrix} M - \frac{k}{2}L^f & \frac{k}{2}M^s & 0\\ \frac{1}{2}\frac{\partial \left(N_1 + S^s + S^f\right)}{\partial u_h} + k\frac{\partial B}{\partial u_h}p_h & M^s + \beta M^f \frac{k}{2}\frac{\partial N_2}{\partial v_h} + \frac{k}{2}\frac{\partial \left(N_1 + S_f^2\right)}{\partial v_h} & kB\\ B^{sT} + \frac{\partial B^{fT}}{\partial u_h}v_h & B^{fT} & 0 \end{bmatrix}$$

$$\begin{bmatrix} S_{uu} & S_{uv} & 0\\ S_{vu} & S_{vv} & kB\\ c_u B^{sT} & c_v B^{fT} & 0 \end{bmatrix} \begin{bmatrix} u\\ v\\ p \end{bmatrix} = \begin{bmatrix} f_u\\ f_v\\ f_p \end{bmatrix}$$

Typical discrete saddle point problem as well known for incompressible NSE



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• Structure part

$$\frac{\partial v^s}{\partial t} = \nabla \cdot \left(J \sigma^s F^{-T} \right) f, \quad det(F) = 1 \quad \text{in } \Omega^s$$
$$u^s = 0, \quad \sigma^s n = 0 \quad \text{on } \Gamma^3$$

• Interface

$$v^f = v^s, \quad \sigma^f n = \sigma^s n \quad \text{on } \Gamma^0_t$$



Governing equations



- Fluid part
 - **Generalized Navier-Stokes equations**

$$\rho \frac{\partial v}{\partial t} + v \cdot \nabla v - \nabla \cdot \sigma + \nabla p = \rho f \quad , \quad \nabla \cdot v = 0,$$
$$\frac{\partial \Theta}{\partial t} + v \cdot \nabla \Theta - \nabla \cdot (k \nabla \Theta) = D : \sigma,$$
$$\sigma = \sigma^s + \sigma^p \quad , \quad D = \frac{1}{2} \left(\nabla v + (\nabla v)^T \right).$$

/iscous stress
$$\sigma^s = 2n_s (D\pi, \Theta) D \quad , \quad D\pi = tr(D^2).$$

- V $O = 2\eta_s(D_{\mathrm{II}}, \Theta)D \quad , \quad D_{\mathrm{II}} = U(D).$
- $\sigma^p + \Lambda \frac{\delta_a \sigma^p}{\delta t} = 2\eta_p D,$ **Elastic stress**



Numerical Methods

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- **FEM-Discretization**
 - The quadriplex FE $Q_2/Q2/P_1^{disc}/Q2$ for displacement-velocity-pressure-stress
 - Edge-oriented stabilization for
 - convective dominated problem
 - > equal interpolation for stress and velocity (special models)
- LCR formulation
 - Conformation tensor is positive

$$\tau(X,t) = \int_{\infty}^{t} \frac{\eta_p}{\Lambda} \exp\left(\frac{-(t-s)}{\sqrt{\Lambda}}\right) F(s,t) F(s,t)^{\mathrm{T}} ds$$

• Positivity preserving via the change of variable

$$\left(\frac{\partial}{\partial t} + u \cdot \nabla\right) \tau - (\Omega \tau - \tau \Omega) + 2 B \tau = \frac{1}{\Lambda} (1 - \tau)$$



Solvers



- Inexact Newton
 - The Jacobian matrix is approximated using finite differences

$$\left[\frac{\partial R(\mathbf{x}^n)}{\partial \mathbf{x}}\right]_{ij} \approx \frac{R_j(\mathbf{x}^n + \epsilon e_j) - R_i(\mathbf{x}^n - \epsilon e_i)}{2\epsilon}$$

- Multgrid Solver
 - Local MPSC via Vanka-like smoother

$$\begin{bmatrix} u^{l+1} \\ v^{l+1} \\ \sigma^{l+1} \\ \Theta^{l+1} \\ p^{l+1} \end{bmatrix} = \begin{bmatrix} u^l \\ v^l \\ \sigma^l \\ \Theta^l \\ p^l \end{bmatrix} + \omega^l \begin{bmatrix} (K+J)_{|T} \end{bmatrix}^{-1} \begin{bmatrix} Res_u \\ Res_v \\ Res_\sigma \\ Res_\Theta \\ Res_p \end{bmatrix}_{|T|}$$

Viscoelastic benchmark



• Planar flow around cylinder (Oldroyd-B)









Parameter	FSI1	FSI2	FSI3
ρ^{s} [10 ³ kg/m ³]	1	1	1
	0.4	0.4	0.4
$\mu^{s}[10^{6}\mathrm{kg/ms}^{2}]$	0.5	0.5	2.0
$\rho^{s}[10^{3} \text{kg/m}^{3}]$	1	1	1
$v^{s}[10^{-3}m^{2}/s]$	1	1	1
$\overline{U}[m/s]$	0.2	1	2

Parameter	FSI1	FSI2	FSI3
$\beta = \frac{\rho^{s}}{\rho^{f}}$ $Ae = \frac{E^{s}}{\rho^{f} \overline{U}^{2}}$	1	1	1
	0.4	0.4	0.4
$Re = \frac{\overline{U}d}{v^{f}}$ $\overline{U}[m/s]$	20	100	200
	0.2	1	2

> FSI1: steady, small deformations



	ux of A $[x 10^{-3}m]$	uy of A $[\times 10^{-3}m]$	drag	lift	
FSI1	0.0227	0.8209	14.295	0.7638	GFD



FSI2: large deformations, periodical oscillations



Test	ux of A $[x 10^{-3}m]$	uy of A $[x 10^{-3}m]$	drag	lift 🌔 🥂	
FSI2	$-14.58 \pm 12.44[3.8]$	$1.23 \pm 80.6[2.0]$	208.83 ± 73.75[3.8]	$0.88 \pm 234.2[2.0]$	CFD



> FSI3: large deformations, complex oscillations



FSI4: benchmarking of experimental data

Flustruc experiment, Erlangen, http://www.lstm.uni-erlangen.de/flustruc



fluid parameters	
density of the fluid	1.05e-6 [kg/mm^3]
kinematic viscosity	164.0

solid parameters	
density of the beam (steel)	7.85e-6[kg/mm^3]
density of the rear mass	7.8e-6 [kg/mm^3]
shear modulus	7.58e13
poisson ratio	0.3



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> FSI4: benchmarking of experimental data

- + Laminar Flow (glycerine)
- + "2D" flow and deformation
- Rotational degree of freedom
- Large aspect ratio (thin structure)
- Corners









Brain Aneurysms and stent implants

Aim: Numerical study of FSI due to stent geometries <u>and</u> elastic wall behaviour



Mesh for numerical Simulation

Cerebral aneurysm





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Aneurysm (pulsatile inflow)

Strong influence of stent geometry and elastic wall deformations



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New Numerical and Algorithmic tools are available using

- Monolithic Finite Element Method
- Arbitrary Lagrangian-Eulerian Formulation
- LCR for viscoelastic flow
- ✓ EO-FEM stabilization
- ✓ Fast Multigrid Solver with local MPSC smoother

For the simulation of FSI with application to hemodynamics

